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4-5-2019

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### Recommended Citation

Hoyt, Catherine R.; Van, Andrew N.; Ortega, Mario; Koller, Jonathan M.; Everett, Elyse A.; Nguyen, Annie L.; Lang, Catherine E.; Schlaggar, Bradley L.; and Dosenbach, Nico U.F., "Detection of pediatric upper extremity motor activity and deficits with accelerometry." JAMA Network Open. 2, 4. e192970 (2019). [https://digitalcommons.wustl.edu/open\\_access\\_pubs/8924](https://digitalcommons.wustl.edu/open_access_pubs/8924)

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## Original Investigation | Pediatrics

# Detection of Pediatric Upper Extremity Motor Activity and Deficits With Accelerometry

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## Abstract

**IMPORTANCE** Affordable, quantitative methods to screen children for developmental delays are needed. Motor milestones can be an indicator of developmental delay and may be used to track developmental progress. Accelerometry offers a way to gather real-world information about pediatric motor behavior.

**OBJECTIVE** To develop a referent cohort of pediatric accelerometry from bilateral upper extremities (UEs) and determine whether movement can accurately distinguish those with and without motor deficits.

**DESIGN, SETTING, AND PARTICIPANTS** Children aged 0 to 17 years participated in a prospective cohort from December 8, 2014, to December 29, 2017. Children were recruited from Ranken Jordan Pediatric Bridge Hospital, Maryland Heights, Missouri, and Washington University School of Medicine in St Louis, St Louis, Missouri. Typically developing children were included as a referent cohort if they had no history of motor or neurological deficit; consecutive sampling and matching ensured equal representation of sex and age. Children with diagnosed asymmetric motor deficits were included in the motor impaired cohort.

**EXPOSURES** Bilateral UE motor activity was measured using wrist-worn accelerometers for a total of 100 hours in 25-hour increments.

**MAIN OUTCOMES AND MEASURES** To characterize bilateral UE motor activity in a referent cohort for the purpose of detecting irregularities in the future, total activity and the use ratio between UEs were used to describe typically developing children. Asymmetric impairment was classified using the mono-arm use index (MAUI) and bilateral-arm use index (BAUI) to quantify the acceleration of unilateral movements.

**RESULTS** A total of 216 children enrolled, and 185 children were included in analysis. Of these, 156 were typically developing, with mean (SD) age 9.1 (5.1) years and 81 boys (52.0%). There were 29 children in the motor impaired cohort, with mean (SD) age 7.4 (4.4) years and 16 boys (55.2%). The combined MAUI and BAUI (mean [SD], 0.86 [0.005] and use ratio (mean [SD], 0.90 [0.008]) had similar F1 values. The area under the curve was also similar between the combined MAUI and BAUI (mean [SD], 0.98 [0.004]) and the use ratio (mean [SD], 0.98 [0.004]).

**CONCLUSIONS AND RELEVANCE** Bilateral UE movement as measured with accelerometry may provide a meaningful metric of real-world motor behavior across childhood. Screening in early childhood remains a challenge; MAUI may provide an effective method for clinicians to measure and visualize real-world motor behavior in children at risk for asymmetrical deficits.

JAMA Network Open. 2019;2(4):e192970. doi:10.1001/jamanetworkopen.2019.2970

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## Key Points

**Question** Can accelerometry be used to measure typical development and identify motor deficits in childhood?

**Findings** In this cohort study of 185 children aged 0 to 17 years, age was a significant predictor of total activity as measured by bilateral upper extremity accelerometry. The mono-arm use index, which provides clinically relevant visualization of asymmetric impairment, is described.

**Meaning** Bilateral upper extremity accelerometry is an affordable, efficient method to objectively measure real-world movement to identify motor aberrancies in childhood.

+ [Video](#)

+ [Supplemental content](#)

Author affiliations and article information are listed at the end of this article.

## Introduction

Developmental delays affect approximately 1 in 6 children in the United States and are a common medical issue seen by pediatric primary care professionals.<sup>1</sup> The costs associated with disability are substantial and continue throughout life.<sup>2,3</sup> To improve long-term outcomes, standard care has incorporated early developmental screening of infants and young children, leading to increased identification of delays and subsequent referral to appropriate services.<sup>4,5</sup> Developmental delays in the first years of life can be subtle, difficult to detect by parents, and not immediately obvious in brief clinical encounters.<sup>6-12</sup> Improving methods for the early detection of deficits would allow for earlier intervention during critical periods of rapid development and thus could reduce disability and associated costs.<sup>13</sup>

Motor development is the earliest observable benchmark of developmental progress because of its rapid, predictable advancement in young children. Developmental milestones in other domains are not as easily tracked and are difficult to measure at young ages.<sup>14</sup> Arguably, then, motor development is the best target for early identification of more widespread disability. Yet accurate measurements of real-world motor behavior have been challenging. Hence, simple, affordable, and quantitative measurements of movement using wearable biosensors, such as accelerometers, during childhood could improve pediatric screenings for developmental delays.

Wearable technology is quickly becoming part of everyday life and has opened the possibility to objectively measure real-world behavior outside of the clinical environment.<sup>15</sup> Wearable biosensors that measure acceleration allow for easy collection of large amounts of data about an individual's activity.<sup>16-18</sup> Accelerometry research in adults suggests it is reliable and valid<sup>16,19-22</sup> with potential clinical relevance.<sup>23</sup> Capturing real-world activity with accelerometers could be especially valuable for pediatric patients, as they often behave differently in the clinical setting.<sup>24,25</sup> The potential for accelerometry in pediatrics has been recognized but has largely been limited to tracking physical activity and sleep disturbances,<sup>26-33</sup> often relying on short wearing periods and hip-worn sensors in small patient populations.<sup>34,35</sup> Accelerometers have not yet been used to detail typical motor development, to our knowledge.

Apart from accurately measuring general activity levels, we hypothesize that bilaterally worn accelerometers can also detect asymmetries in motor patterns. Deficits affecting one side of the body, or hemiparesis, constitute the most common form of cerebral palsy (CP), which is the most common cause of pediatric disability.<sup>36,37</sup> Therefore, the early identification of real-life motor asymmetries could greatly facilitate diagnosis and treatment for this population. Conversely, children with identified brain injury (eg, perinatal stroke) are presumed to need rehabilitation services, although some have no neurological deficits. To date, there is limited ability to measure the real-world upper extremity (UE) activity with high interrater reliability.<sup>38</sup> Previous methods that have analyzed UE movement have calculated the ratio of total frequency of movement of each UE, which can provide valuable information in adults or typically developing children.

In children, wrist-worn accelerometers encourage greater adherence and provide more accurate information about physical activity than hip-worn sensors.<sup>39</sup> Collecting data during the course of several complete days on bilateral wrists from a referent cohort would allow for comparison between populations and the identification of children with aberrant motor patterns. Expanding the use of accelerometers to routine clinical care in populations at risk for motor and other developmental delays would provide greater understanding of children's daily activity, allowing primary care professionals to address concerns quickly and with targeted interventions.

The purpose of this study was 2-fold: first, to gather and analyze bilateral UE accelerometry data from a referent cohort of children with typical motor development, and second, to test the validity of the referent bilateral UE accelerometry to discriminate between children with and without motor deficits. Since CP is the most common cause of motor disability in childhood and asymmetric deficits are the most common subtype of CP, we hypothesized that examining bilateral UE data and comparing them with unilateral UE movements would facilitate identification and diagnosis.

Our referent pediatric accelerometry (PEAC) data set represents more than 14 000 hours (561 days) from 156 children aged 0 to 17 years and provides a critical foundation for future studies to describe activity across childhood. Children with hemiparesis have asymmetric deficits that are obscured by traditional analysis and visualization methods, so we propose a new metric to separate unilateral and bilateral movement and incorporate acceleration of movement to more accurately describe the association of asymmetric deficits with real-world UE behavior, which may help classify children who would most benefit from intensive interventions. Isolating unilateral movements using the mono-arm use index (MAUI) should be able to objectively classify indicators for motor disability that are otherwise missed.

## Methods

The Human Research Protection Office of Washington University School of Medicine in St Louis approved this study. A prospective, observational cohort design was used to measure bilateral UE activity in 2 groups of children aged 0 to 17.11 years; children who were developing typically (referent cohort) and children with a diagnosis of asymmetric motor impairment (CP cohort) were recruited from December 8, 2014, to December 29, 2017. Parents provided written informed consent and children older than 7 years provided written assent. Children were asked to wear bilateral UE accelerometers for four 25-hour periods within 1 month. Child behavior, medical history, and demographic data were collected via parent report and managed using Research Electronic Data Capture tools.<sup>40</sup> This study is reported following the Strengthening the Reporting of Observational Studies in Epidemiology (STROBE) reporting guideline.

## Participants and Procedures

Pediatric accelerometry participants were recruited using snowball sampling,<sup>41</sup> in which consented individuals referred research members to other potential participants. Consecutive sampling and matching were used to ensure equal representation of age and sex, with a minimum of 8 children per age year. Children were included if they were typically developing with no significant medical history affecting motor development. Children with structural brain disease, neurological impairment, or autism spectrum disorder were excluded.

To confirm typical development, parents completed either the Movement Assessment Battery for Children-2 Checklist<sup>42</sup> for children 5 years or older or the motor subscales of the Ages and Stages Questionnaire<sup>43</sup> for children younger than 5 years. In addition to motor screening, the Child Behavior Checklist<sup>44</sup> was completed for children older than 18 months. Scores from these measures were compared with published age norms. Parents of typically developing children older than 5 years completed the Participation and Environment Measure for Children-Youth<sup>45,46</sup> to capture typical daily activities.

Participants with confirmed asymmetric motor deficits associated with CP were recruited through the pediatric neurology department at Washington University School of Medicine in St Louis, St Louis, Missouri, and Ranken Jordan Pediatric Bridge Hospital, Maryland Heights, Missouri. Children were excluded if they had autism spectrum disorder, received botulinum toxin therapy in the previous 3 months, or had undergone an orthopedic surgical procedure in the previous 6 months. We aimed to recruit at least 20 participants with hemiplegic CP classified by a gross motor function classification scale<sup>47</sup> score of 1 or 2.

A pediatric occupational therapist assessed UE function of children to confirm asymmetric deficits using standardized assessment tools (eMethods in the [Supplement](#)). The Child Behavior Checklist<sup>44</sup> was completed for children older than 18 months.

## Measurement of Bilateral Upper Extremity Activity

The ActiGraph wGT3X (ActiGraph LLC) is an accelerometer commonly used in pediatric research<sup>48</sup> and was selected for this study because of its durability, long battery life, and water resistance.

Children wore accelerometers bilaterally, just above the ulnar styloid, for four 25-hour periods within 1 month, with movement sampled at 30 Hz. The first and last 30 minutes of data were removed from each 25-hour period to allow for children getting used to the devices or taking them off a few minutes early. Children with at least 72 hours of recorded data were included in analysis (eMethods in the [Supplement](#)). By plotting the variance over the number of samples collected, we determined that 4 days was sufficient for stability of the activity count measurements (eFigure 1 in the [Supplement](#)). A single vector magnitude was calculated for each second by combining activity counts across axes (activity counts =  $\sqrt{x^2 + y^2 + z^2}$ ) and the resulting value was stored as activity counts (1 count = 0.001664g) in 1-second epochs and used for subsequent processing.<sup>49</sup> Data were visually inspected in 30-minute increments for irregularities in activity counts or wear time to identify potential errors in data collection. Parents reported hand dominance of the child at the time of recruitment or close to the child's third birthday.

## Data Processing and Analysis

Accelerometry data were processed using MATLAB version 2015a (The MathWorks Inc) and Python version 3.6 (Python Software Foundation). Periods of movement were determined using previously described methods.<sup>22</sup>

### Referent Cohort

Total activity was calculated by summing the seconds in which the activity count was greater than 10 for each UE. The sum from the dominant UE was used to calculate the total hours of activity for each 24-hour period. Methods for describing UE use and characterizing asymmetric deficits have traditionally relied on a ratio of the sum of seconds of movement of both UE, called the *use ratio* (UR). To characterize the contribution of each UE on a second-by-second basis, we calculated the UR, magnitude ratio, and the bilateral magnitude (eMethods in the [Supplement](#)).

### Cerebral Palsy Cohort

The UR classifies each second as either movement or nonmovement. Using this parameter, bilateral contributions gain equal representation in the dominant/nondominant parts of the ratio, driving the value of the UR toward 1. Thus, the UR is a representation of unilateral movement and may be less sensitive to more subtle deficits because of its inclusion of bilateral data, which tend to be more frequent. Because we aimed to identify asymmetrical use of the UEs, a new, more sensitive metric was developed. The MAUI and bilateral-arm use index (BAUI) include the acceleration of movement such that the intensity of the movement is also taken into account, rather than the mere presence of activity. We also split the unilateral and bilateral contributions into separate indices to provide a more representative evaluation of the data.

### Equations

Mono-arm use index and BAUI can be expressed with the following equations:

$$MAUI = \frac{\sum_{n \in N, A_{dom}(n) = 0} A_{nondom}(n)}{\sum_{n \in N, A_{nondom}(n) = 0} A_{dom}(n)}$$

$$BAUI = \frac{\sum_{n \in N, A_{dom}(n) \neq 0} A_{nondom}(n)}{\sum_{n \in N, A_{nondom}(n) \neq 0} A_{dom}(n)}$$

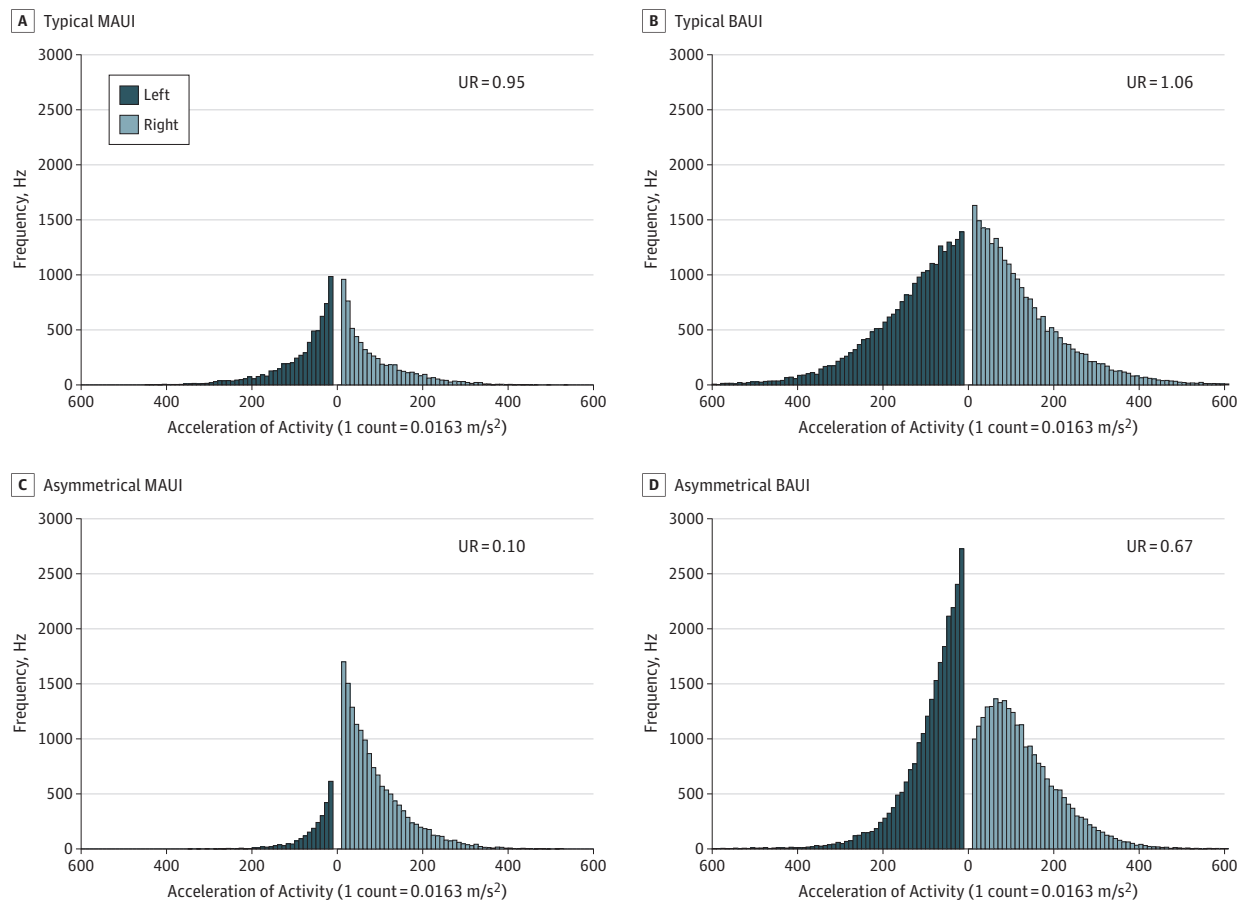
The sample,  $n$ , represents a single sample in the total number of samples,  $N$ . The activity count,  $A$ , represents the activity of the individual at a particular  $n$  and is separated between the dominant and nondominant extremities. By summing the activity counts across each extremity through each conditional sum, the use index,  $R$ , for the bilateral and unilateral contributions is obtained.

The MAUI reflects the ratio of the sum of the magnitude of all independent movements of each arm. The BAUI reflects the ratio of the total intensity of bilateral UE movements. The MAUI more accurately describes the extent of deficit by objectively measuring the effort of each arm and quantifying the frequency of independent movement in everyday activities (eg, texting, opening doors). The UR obscures potentially informative data and is often visualized with complicated 3-dimensional plots. As illustrated in **Figure 1**, the MAUI and BAUI metrics provide an intuitive solution to visualize an individual's movement that is missed using the UR.

Statistical Analysis

Analyses were completed using R version 3.5.3 (R Project for Statistical Computing). The 2 cohorts were compared by age (*t* test), sex ( $\chi^2$  test), and handedness (Fisher exact test). Total activity was summed for each day of accelerometry data and the UR between UE was calculated. A general additive model was used to curve fit the data and summary statistics were calculated. For the referent cohort, the mean and SD were calculated to summarize the UR and UE activity for each age year. The median magnitude ratio and bilateral magnitude were calculated for each age year. The magnitude ratio was calculated for each second of data by taking the natural log of the vector magnitude of the nondominant UE and dividing it by the vector magnitude of the dominant UE; a magnitude ratio of 0 reflects equal contribution from both UEs.<sup>21,50</sup> The bilateral magnitude denotes the intensity of activity on a second-by-second basis by summing the vector magnitude of both the dominant and nondominant UEs; a bilateral magnitude of 0

Figure 1. Activity From Upper Limbs in a Typically Developing Child and a Child with Asymmetric Deficits



Histograms representing activity from both upper limbs in bins of 10 during 24 hours and representing two 8-year-old girls. A and B, Typically developing child who uses both limbs equally. C and D, A child with cerebral palsy. Her right hand is used more for

independent movement (C), and her left upper limb is used predominantly in low-intensity bilateral movement (D). BAUI indicates bilateral-arm use index; MAUI, mono-arm use index; UR, use ratio.

reflects no activity.<sup>21,50</sup> To describe differences in UE use, unpaired *t* tests were used to compare children older than 36 months (presumed handedness) with children younger than 36 months. To compare between the PEAC referent cohort and children with motor deficits, the MAUI and BAUI indices were calculated. We compared the performance of our proposed MAUI and BAUI metrics with the UE UR using logistic regression classification. To validate our model, we used stratified nested *k* × *l*-fold cross validation (*k* = 7, *l* = 7) for 30 trials, which was selected for computational tractability. For each trial, we recorded the mean F1 scores (measure of accuracy relying on precision and recall) and the area under the curve across the 7 *k*-folds. Then, the SD was calculated across trials to determine the effectiveness of using MAUI to accurately discriminate between those with and without asymmetric motor deficits.

## Results

### Participant Characteristics

Two cohorts were recruited for this study. A total of 216 children enrolled and 185 children were included in the analyses. The data for the PEAC cohort and associated code are publicly available online.<sup>51</sup> The **Table** presents demographic information for both cohorts. Groups differed in in age

**Table. Characteristics of Participants**

Characteristic	No. (%)	
	Typically Developing (n = 156)	Motor Impaired (n = 29)
<b>Children</b>		
Boys	81 (52)	16 (55)
Age, mean (SD), mo	109 (61.61)	89 (52.7)
Right hand dominance	147 (94)	7 (24)
Race/ethnicity <sup>a</sup>		
White	141 (90)	27 (93)
Multiracial	9 (6)	0
African American	4 (3)	0
Asian	2 (1)	1 (3)
Hispanic or Latino	1 (1)	2 (7)
Not reported	0	1 (3)
Developmental score outside of clinical norms		
MABC <sup>b</sup>	2 (1)	NA
ASQ <sup>b</sup>	2 (1)	NA
CBCL <sup>c</sup>	4	5
Not reported	6 (4)	NA
<b>Parents</b>		
<b>Marital status</b>		
Married	137 (88)	25 (86)
Divorced or separated	11 (7)	2 (7)
Single or not married	8 (5)	2 (7)
<b>Maternal educational level</b>		
Doctoral or professional degree	58 (37)	0
Bachelor's or master's degree	84 (54)	21 (72)
Associate degree or some college	13 (8)	6 (21)
High school diploma or GED equivalent	1 (0.1)	0
<b>No. of children in home</b>		
≥3	64 (41)	9 (31)
2	56 (36)	12 (41)
1	20 (13)	7 (24)
0 or not reported	16 (10)	1 (3)

Abbreviations: ASQ, Ages and Stages Questionnaire, fine and gross motor subtests for children age 0 to 5 years; CBCL, Child Behavior Checklist for children older than 5 years; GED, General Education Development; MABC, Movement Assessment Battery for Children Checklist for ages older than 5 years; NA, not applicable.

<sup>a</sup> Race/ethnicity was self-reported. Participants were allowed to select Hispanic or Latino in addition to race/ethnicity, explaining why sum is more than 100%.

<sup>b</sup> Parents completed surveys to confirm typical development.

<sup>c</sup> Child Behavior Checklist for children older than 5 years; total scores greater than 2-fold SD were considered abnormal.



( $t = -2.77$ ;  $P = .006$ ) and handedness ( $P < .001$  by Fisher exact test), but did not differ with respect to sex ( $\chi^2_1 = 2.37$ ;  $P = .12$ ).

### Referent Cohort (PEAC)

Of the 176 typically developing children who were enrolled in the PEAC cohort, data from 2 participants were removed, 1 child for inaccurate device placement and 1 child because of observed developmental delay by one of us (C.R.H.). An additional 18 participants were removed because of insufficient data caused by suspected device malfunctioning, discrepancy between right and left recording length, or wear time. In the referent cohort, 156 children were included in analysis. The mean (SD) age was 9.1 (5.1) years, and there were 81 boys (52.0%). Overall, parents reported that their children participated predominantly in sedentary activities (eFigure 2 in the [Supplement](#)).

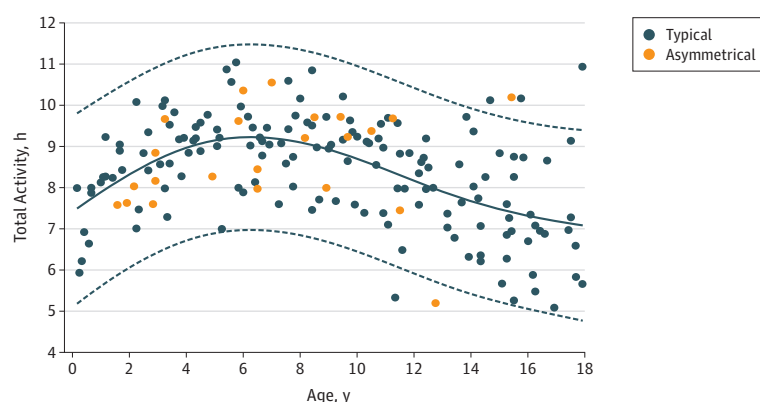
**Figure 2** illustrates the developmental curve using a general additive model with cubic smoothing splines of real-life daily activity, in which age was a significant predictor of total activity ( $F = 28.2$ ,  $R^2 = 0.16$ ,  $P < .001$ ). Objective measurement of total activity across childhood in typically developing children is critical for beginning to understand changes in both active and sedentary behavior.

The decline of the UE UR reported in **Figure 3A** represents the first objective measurement of bilateral UE use across childhood, to our knowledge. Children at the youngest end of the cohort had a mean UR of 1, which declined in the first years of life to reach adult norms by adolescence and can be observed in the MAUI ratio of typically developing children as they age (**Video 1**). The difference in UR between those with and without hand dominance (cutoff for handedness was set at 36 months) was statistically significant ( $t = -3.83$ ,  $P < .001$ ). These findings correspond with the age range when hand dominance is considered to emerge and solidify.<sup>52</sup> Total activity hours and counts, UR, magnitude ratio, and bilateral magnitude are reported for each age year in the eTable in the [Supplement](#).

### Cerebral Palsy Cohort

Of the 40 children recruited for the CP cohort, 29 participants were included in the analysis. The mean (SD) age was 7.4 (4.4) years and 16 (55.2%) were boys. Participants were excluded if there were insufficient data (<72 hours). All motor deficits were associated with hemiplegic CP (gross motor function classification score of 1 or 2) due to various etiologies (eFigure 3 in the [Supplement](#)). Nine children (31%) were born prematurely, and 12 children (41%) had a documented learning disability. Children with asymmetric impairment demonstrated similar total activity to their typically developing peers (**Figure 2**) but used their dominant hands significantly more, which is observable in the differences in UR in **Figure 3B**. The combined MAUI and BAUI metric had a larger margin of separation when compared with the UR, with more differentiation carried by the MAUI metric (**Figure 4**). As seen in **Figure 1**, this separation can be easily visualized in individuals with asymmetric impairment. Using a logistic regression model (**Figure 4**) validated with our  $k \times l$ -fold cross validation,

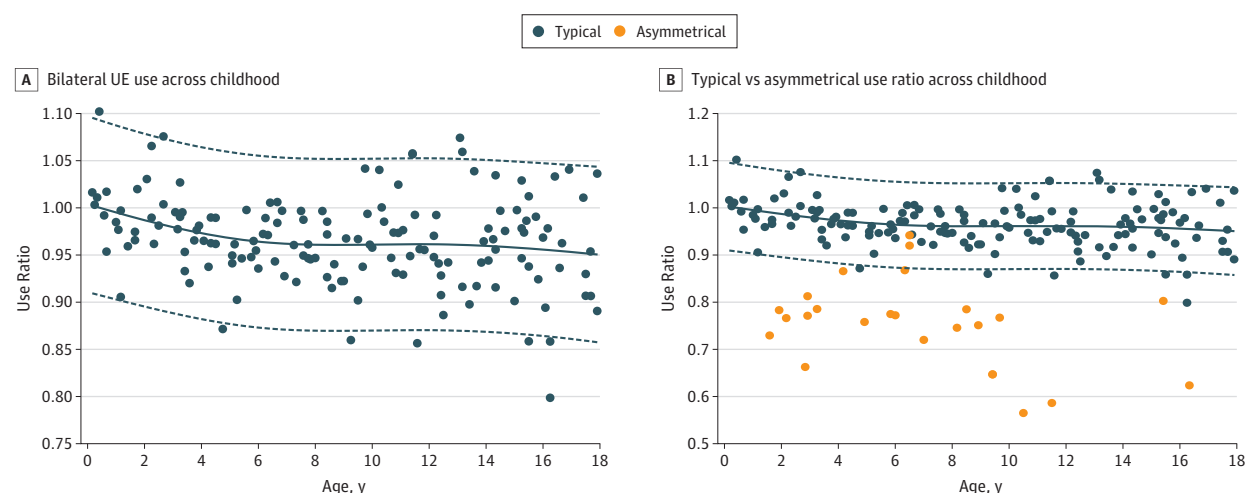
Figure 2. Upper Limb Movement of Measured With Bilateral Accelerometers



Plot shows the association of age with total daily activity, measured in 1-second epochs. Each point represents a 24-hour period. The solid line represents a local regression fit of all visits using a general additive model, and dashed lines represent 95% CI.

we compared the effectiveness of the UR metric with the combined MAUI and BAUI metric. The combined MAUI and BAUI metric (mean [SD], 0.86 [0.005]) and UR (mean [SD], [0.008]) had comparable F1 values. The area under the curve was also comparable between the combined MAUI and BAUI metric (mean [SD], 0.98 [0.004]) and UR (mean [SD], 0.98 [0.004]). Video analysis from the Melbourne Assessment demonstrated that children misclassified by MAUI did not have measurable deficits impairing UE activity, as visualized with the child in **Video 2**, with Melbourne domain scores ranging from 85% to 100% (not significantly impaired). The MAUI demonstrated that children with asymmetric motor deficits used their dominant arms much more than their affected arms. We did not impose a minimum amount of total unilateral activity, which is the basis of the MAUI analysis. Therefore, since unilateral movement is a subset of total activity, variance across days was higher than for the total UR.

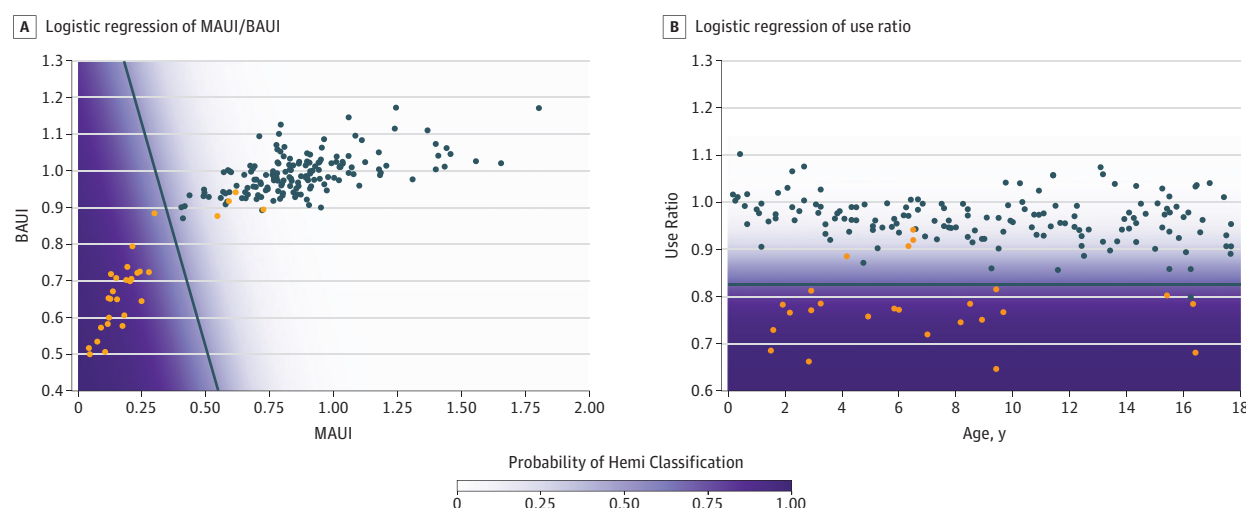
Figure 3. Use Ratio of Total Activity of Upper Limbs in Children Aged 0 to 17 Years



Solid line represents a local regression of all pediatric accelerometry visits, and dashed lines represent 95% CI (referent cohort). A, Mean upper extremity use ratio declined in years of life. The decline demonstrated increased use of a dominant upper limb in

typically developing children. B, Use ratio was lower for children with asymmetric impairment. Points within the 95% CI represent children without significant impairment (**Video 2**). UE indicates upper extremity.

Figure 4. Unilateral and Bilateral Movements and Use Ratios Between Groups



A, Using the mono-arm use index (MAUI) and bilateral-arm use index (BAUI) metric found an F1 score of 0.92 (SD, 0.008) and area under the curve of 0.98 (SD, 0.004). B, Using the use ratio methods from Bailey and Lang<sup>22</sup> with the same data, there was an F1 score of 0.90 (SD, 0.008) and area under the curve of 0.98 (SD, 0.004).

## Discussion

This study provides preliminary data that bilateral UE accelerometry can track typical childhood motor development and be used to discriminate those with subtle asymmetric motor impairments in CP. Given the importance of early diagnosis and the challenges associated with current screening methods, a reliable method for objectively measuring real-world motor behavior that is clinically useful is greatly needed. Our novel approach of measuring activity on bilateral UE in children using single-use bracelets had several important advantages. Primarily, we were able to acquire data continuously through all activities of daily living and eliminate participants having to remember to don devices following bathing or sleeping. Our findings provide promising evidence that wearable technology can provide medically important information across childhood, creating the possibility to screen at-risk populations (eg, premature infants) and determine the extent that brain injury may have affected real-world movement, helping to determine the need for intervention. Further, our measurement of bilateral activity in typically developing children allowed us to compare pediatric populations for the first time, to our knowledge, establishing that our cohort of children with asymmetric impairment had total activity that fell within normal limits compared with the PEAC cohort. Our comparison between UEs using the UR provided a clear indication that, while total activity have been similar, children with asymmetric impairment used their dominant hands more frequently and that our MAUI metric of the independent UE movements would provide a more accurate picture of UE motor disability.

Another important finding from this study is that accelerometry measured with wearable devices may provide a quantitative method to track developmental trajectories, such as the emergence of handedness, in addition to providing a useful clinical tool to describe real-world motor behavior and its association with child development. While it is possible to observe strong hand preferences at early ages, subtle differences in UE use are often difficult to identify. The low cost and low participant burden of wearable technology present an exciting opportunity to measure real-world motor behavior in the clinical setting.<sup>15</sup> Using bilateral UE accelerometers greatly improved measurement of childhood motor activity by increasing the quality of our data (comparing UEs) and simultaneously providing the ability to track the UR across ages.

## Limitations

The present study was an observational cohort investigation of children with inherent limitations. To recruit this large cohort and meet family constraints, we were often reliant on parents to properly affix the accelerometers on their children. Although we are confident in the presented results, it is possible that accelerometers were used incorrectly. To meet recruitment goals, children were categorized by their age year, which limits analyses of discrete changes, especially in early childhood when development is rapid. Although we were cautious about not overfitting the data, it is possible that the reported efficacy of this model is optimistic. As is required for many developmental curves, a larger cohort of children in the first 2 years of life should be considered for future studies. Future studies should bolster the younger cohorts to get a better idea of when hand dominance emerges, if it can be reliably identified, and if disability can be predicted with accelerometry. Accelerometry data collected from children who participate in sports would further benefit future studies describing typical activity in older children.

## Conclusions

This is the first study to use accelerometers to measure activity from birth to adulthood and separate unilateral and bilateral movement, to our knowledge. The UR provides important information about UE activity. However, our findings indicate that separating the unilateral and bilateral movements using MAUI and BAUI metrics may be a more efficient method to screen for subtle motor aberrancies in childhood. However, we found that MAUI drives most cases and provides clinically relevant

information that can be readily visualized and interpreted by the health care team to identify children who present with atypical motor patterns. Our findings indicate that our MAUI metric may be a useful tool in pediatric neurologic and rehabilitative care even at very young ages. The misclassified measurements were from children with impairments diagnosed from magnetic resonance imaging findings and who had been referred for intensive unilateral rehabilitation. However, despite neural damage, these children presented motor skills similar to typical peers (**Video 2**), indicating that a costly, time-consuming intervention may not be warranted.

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## ARTICLE INFORMATION

**Accepted for Publication:** March 11, 2019.

**Published:** April 26, 2019. doi:10.1001/jamanetworkopen.2019.2970

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**Conflict of Interest Disclosures:** Dr Lang reported grants from National Institutes of Health during the conduct of the study. Dr Dosenbach reported grants from Kiwanis Neuroscience Research Foundation, the Jacobs Foundation, and the National Institute of Neurological Disorders and Stroke during the conduct of the study. No other disclosures were reported.

**Funding/Support:** This work was supported by the National Institutes of Health (grants NS088590, TRO00448 [Dr Dosenbach], 1P30NS098577 [to the Neuroimaging Informatics and Analysis Center], and HD087011 [to the Intellectual and Developmental Disabilities Research Center at Washington University]); the Jacobs Foundation (grant 2016121703 [Dr Dosenbach]); the Child Neurology Foundation (Dr Dosenbach); the McDonnell Center for Systems Neuroscience (Drs Dosenbach and Schlaggar); the Mallinckrodt Institute of Radiology (grant 14-011 [Dr Dosenbach]); the Hope Center for Neurological Disorders (Drs Dosenbach and Schlaggar); and the Kiwanis Neuroscience Research Foundation (Drs Dosenbach and Schlaggar).

**Role of the Funder/Sponsor:** The funding organizations were not responsible or involved with design and conduct of the study; collection, management, analysis, and interpretation of the data; preparation, review, or approval of the manuscript; or decision to submit the manuscript for publication.

**Additional Contributions:** Sarah E. Sherman, BS, Shelby Brown, BS, and Melanie Berner, MSOT (graduate students, Program in Occupational Therapy, Washington University in St Louis, St Louis, Missouri), contributed to data collection. Dustin K. Ragan, PhD, Sarah J. Gross, BS, Jason Lenox, BS, and Jackie M. Hampton, BS (Washington University School of Medicine in St Louis), contributed to data collection and analysis. None of these individuals received compensation beyond their salaries for their work. We thank the patient in Video 2 for granting permission to publish this information.

## REFERENCES

1. Boyle CA, Boulet S, Schieve LA, et al. Trends in the prevalence of developmental disabilities in US children, 1997-2008. *Pediatrics*. 2011;127(6):1034-1042. doi:10.1542/peds.2010-2989
2. Stabile M, Allin S. The economic costs of childhood disability. *Future Child*. 2012;22(1):65-96. doi:10.1353/foc.2012.0008
3. Korvenranta E, Lehtonen L, Rautava L, et al; PERFECT Preterm Infant Study Group. Impact of very preterm birth on health care costs at five years of age. *Pediatrics*. 2010;125(5):e1109-e1114. doi:10.1542/peds.2009-2882
4. Duby JC, Lipkin PH, Macias MM, et al; Council on Children With Disabilities; Section on Developmental Behavioral Pediatrics; Bright Futures Steering Committee; Medical Home Initiatives for Children With Special Needs Project Advisory Committee. Identifying infants and young children with developmental disorders in the medical home: an algorithm for developmental surveillance and screening. *Pediatrics*. 2006;118(1):405-420. doi:10.1542/peds.2006-1231
5. Schonwald A, Huntington N, Chan E, Risko W, Bridgemohan C. Routine developmental screening implemented in urban primary care settings: more evidence of feasibility and effectiveness. *Pediatrics*. 2009;123(2):660-668. doi:10.1542/peds.2007-2798
6. Bender BG, Bartlett SJ, Rand CS, Turner C, Wamboldt FS, Zhang L. Impact of interview mode on accuracy of child and parent report of adherence with asthma-controller medication. *Pediatrics*. 2007;120(3):e471-e477. doi:10.1542/peds.2006-3457
7. Rydz D, Srour M, Oskoui M, et al. Screening for developmental delay in the setting of a community pediatric clinic: a prospective assessment of parent-report questionnaires. *Pediatrics*. 2006;118(4):e1178-e1186. doi:10.1542/peds.2006-0466
8. Voigt RG, Llorente AM, Jensen CL, Fraley JK, Barbaresi WJ, Heird WC. Comparison of the validity of direct pediatric developmental evaluation versus developmental screening by parent report. *Clin Pediatr (Phila)*. 2007;46(6):523-529. doi:10.1177/0009922806299100
9. Uswatte G, Taub E, Griffin A, Vogtle L, Rowe J, Barman J. The pediatric motor activity log-revised: assessing real-world arm use in children with cerebral palsy. *Rehabil Psychol*. 2012;57(2):149-158. doi:10.1037/a0028516
10. Beckung E, Hagberg G. Neuroimpairments, activity limitations, and participation restrictions in children with cerebral palsy. *Dev Med Child Neurol*. 2002;44(5):309-316. doi:10.1111/j.1469-8749.2002.tb00816.x
11. Taub E, Griffin A, Nick J, Gammons K, Uswatte G, Law CR. Pediatric CI therapy for stroke-induced hemiparesis in young children. *Dev Neurorehabil*. 2007;10(1):3-18. doi:10.1080/13638490601151836
12. First LR, Palfrey JS. The infant or young child with developmental delay. *N Engl J Med*. 1994;330(7):478-483. doi:10.1056/NEJM199402173300708
13. Bellman M, Byrne O, Sege R. Developmental assessment of children. *BMJ*. 2013;346:e8687. doi:10.1136/bmj.e8687
14. Developmental surveillance and screening of infants and young children. *Pediatrics*. 2001;108(1):192-196. doi:10.1542/peds.108.1.192
15. Trost SG, O'Neil M. Clinical use of objective measures of physical activity. *Br J Sports Med*. 2014;48(3):178-181. doi:10.1136/bjsports-2013-093173
16. Uswatte G, Giuliani C, Winstein C, Zeringue A, Hobbs L, Wolf SL. Validity of accelerometry for monitoring real-world arm activity in patients with subacute stroke: evidence from the extremity constraint-induced therapy evaluation trial. *Arch Phys Med Rehabil*. 2006;87(10):1340-1345. doi:10.1016/j.apmr.2006.06.006
17. Gebruers N, Vanroy C, Truijens S, Engelborghs S, De Deyn PP. Monitoring of physical activity after stroke: a systematic review of accelerometry-based measures. *Arch Phys Med Rehabil*. 2010;91(2):288-297. doi:10.1016/j.apmr.2009.10.025
18. Gironde RJ, Lloyd J, Clark ME, Walker RL. Preliminary evaluation of reliability and criterion validity of Actiwatch-Score. *J Rehabil Res Dev*. 2007;44(2):223-230. doi:10.1682/JRRD.2006.06.0058

19. Uswatte G, Miltner WH, Foo B, Varma M, Moran S, Taub E. Objective measurement of functional upper-extremity movement using accelerometer recordings transformed with a threshold filter. *Stroke*. 2000;31(3):662-667. doi:10.1161/01.STR.31.3.662
20. van der Pas SC, Verbunt JA, Breukelaar DE, van Woerden R, Seelen HA. Assessment of arm activity using triaxial accelerometry in patients with a stroke. *Arch Phys Med Rehabil*. 2011;92(9):1437-1442. doi:10.1016/j.apmr.2011.02.021
21. Bailey RR, Klaesner JW, Lang CE. An accelerometry-based methodology for assessment of real-world bilateral upper extremity activity. *PLoS One*. 2014;9(7):e103135. doi:10.1371/journal.pone.0103135
22. Bailey RR, Lang CE. Upper-limb activity in adults: referent values using accelerometry. *J Rehabil Res Dev*. 2013;50(9):1213-1222. doi:10.1682/JRRD.2012.12.0222
23. Lang CE, Bland MD, Bailey RR, Schaefer SY, Birkenmeier RL. Assessment of upper extremity impairment, function, and activity after stroke: foundations for clinical decision making. *J Hand Therapy*. 2013;26(2):104-114 doi:10.1016/j.jht.2012.06.005
24. Rand D, Eng JJ. Disparity between functional recovery and daily use of the upper and lower extremities during subacute stroke rehabilitation. *Neurorehabil Neural Repair*. 2012;26(1):76-84. doi:10.1177/1545968311408918
25. Michielsen ME, Selles RW, Stam HJ, Ribbers GM, Bussmann JB. Quantifying nonuse in chronic stroke patients: a study into paretic, nonparetic, and bimanual upper-limb use in daily life. *Arch Phys Med Rehabil*. 2012;93(11):1975-1981. doi:10.1016/j.apmr.2012.03.016
26. Lin P, Chang KT, Lin YA, Tzeng IS, Chuang HH, Chen JY. Association between self-reported sleep duration and serum lipid profile in a middle-aged and elderly population in Taiwan: a community-based, cross-sectional study. *BMJ Open*. 2017;7(10):e015964. doi:10.1136/bmjopen-2017-015964
27. Taylor RW, Williams SM, Farmer VL, Taylor BJ. Changes in physical activity over time in young children: a longitudinal study using accelerometers. *PLoS One*. 2013;8(11):e81567. doi:10.1371/journal.pone.0081567
28. Williams HG, Pfeiffer KA, O'Neill JR, et al. Motor skill performance and physical activity in preschool children. *Obesity (Silver Spring)*. 2008;16(6):1421-1426. doi:10.1038/oby.2008.214
29. Sadeh A, Lavie P, Scher A, Tirosh E, Epstein R. Actigraphic home-monitoring sleep-disturbed and control infants and young children: a new method for pediatric assessment of sleep-wake patterns. *Pediatrics*. 1991;87(4):494-499.
30. Insana SP, Gozal D, Montgomery-Downs HE. Invalidity of one actigraphy brand for identifying sleep and wake among infants. *Sleep Med*. 2010;11(2):191-196. doi:10.1016/j.sleep.2009.08.010
31. So K, Adamson TM, Horne RSC. The use of actigraphy for assessment of the development of sleep/wake patterns in infants during the first 12 months of life. *J Sleep Res*. 2007;16(2):181-187. doi:10.1111/j.1365-2869.2007.00582.x
32. So K, Buckley P, Adamson TM, Horne RSC. Actigraphy correctly predicts sleep behavior in infants who are younger than six months, when compared with polysomnography. *Pediatr Res*. 2005;58(4):761-765. doi:10.1203/01.PDR.0000180568.97221.56
33. Sung M, Adamson TM, Horne RS. Validation of actigraphy for determining sleep and wake in preterm infants. *Acta Paediatr*. 2009;98(1):52-57. doi:10.1111/j.1651-2227.2008.01002.x
34. Sherar LB, Griew P, Eslinger DW, et al. International children's accelerometry database (ICAD): design and methods. *BMC Public Health*. 2011;11:485. doi:10.1186/1471-2458-11-485
35. Basterfield L, Adamson AJ, Frary JK, Parkinson KN, Pearce MS, Reilly JJ; Gateshead Millennium Study Core Team. Longitudinal study of physical activity and sedentary behavior in children. *Pediatrics*. 2011;127(1):e24-e30. doi:10.1542/peds.2010-1935
36. Cans C; Surveillance of Cerebral Palsy in Europe. Surveillance of cerebral palsy in Europe: a collaboration of cerebral palsy surveys and registers: Surveillance of Cerebral Palsy in Europe (SCPE). *Dev Med Child Neurol*. 2000;42(12):816-824. doi:10.1111/j.1469-8749.2000.tb00695.x
37. Golomb MR, Garg BP, Saha C, Azzouz F, Williams LS. Cerebral palsy after perinatal arterial ischemic stroke. *J Child Neurol*. 2008;23(3):279-286. doi:10.1177/0883073807309246
38. Klingels K, De Cock P, Molenaers G, et al. Upper limb motor and sensory impairments in children with hemiplegic cerebral palsy: can they be measured reliably? *Disabil Rehabil*. 2010;32(5):409-416. doi:10.3109/09638280903171469
39. Fairclough SJ, Noonan R, Rowlands AV, Van Hees V, Knowles Z, Boddy LM. Wear compliance and activity in children wearing wrist- and hip-mounted accelerometers. *Med Sci Sports Exerc*. 2016;48(2):245-253. doi:10.1249/MSS.0000000000000771



40. Harris PA, Taylor R, Thielke R, Payne J, Gonzalez N, Conde JG. Research electronic data capture (REDCap): a metadata-driven methodology and workflow process for providing translational research informatics support. *J Biomed Inform*. 2009;42(2):377-381. doi:10.1016/j.jbi.2008.08.010
41. Goodman LA. Snowball sampling. *Ann Math Statist*. 1961;32(1):148-170. doi:10.1214/aoms/1177705148
42. Henderson SE, Sugden DA, Barnett A. *Movement Assessment Battery for Children*. 2nd ed. London, UK: Pearson Clinical; 2007.
43. Squires J, Twombly E, Bricker D, Potter L. *Ages and Stages Questionnaire 3 User's Guide*. 3rd ed. Baltimore, MD: Brookes Publishing; 2009.
44. Achenbach TM, Rescorla LA. *Manual for the ASEBA School-Age Forms & Profiles*. Burlington: University of Vermont, Research Center for Children, Youth, and Families; 2001.
45. Coster W, Bedell G, Law M, et al. Psychometric evaluation of the Participation and Environment Measure for Children and Youth. *Dev Med Child Neurol*. 2011;53(11):1030-1037. doi:10.1111/j.1469-8749.2011.04094.x
46. Coster W, Law M, Bedell G, Khetani M, Cousins M, Teplicky R. Development of the Participation and Environment Measure for Children and Youth: conceptual basis. *Disabil Rehabil*. 2012;34(3):238-246. doi:10.3109/09638288.2011.603017
47. Palisano R, Rosenbaum P, Walter S, Russell D, Wood E, Galuppi B. Development and reliability of a system to classify gross motor function in children with cerebral palsy. *Dev Med Child Neurol*. 1997;39(4):214-223. doi:10.1111/j.1469-8749.1997.tb07414.x
48. Trost SG, McIver KL, Pate RR. Conducting accelerometer-based activity assessments in field-based research. *Med Sci Sports Exerc*. 2005;37(11 suppl):S531-S543. doi:10.1249/01.mss.0000185657.86065.98
49. Peach D, Van Hoomissen J, Callender HL. Exploring the ActiLife® filtration algorithm: converting raw acceleration data to counts. *Physiol Meas*. 2014;35(12):2359-2367. doi:10.1088/0967-3334/35/12/2359
50. Bailey RR, Klaesner JW, Lang CE. Quantifying real-world upper-limb activity in nondisabled adults and adults with chronic stroke. *Neurorehabil Neural Repair*. 2015;29(10):969-978. doi:10.1177/1545968315583720
51. Hoyt CR, Van AN, Ortega M. Pediatric bilateral upper extremity accelerometry data. <https://wustl.box.com/s/7xr39fkjoowxvwbntroq7po4vwl27he>. Accessed March 22, 2019.
52. van Wely L, Becher JG, Balemans AC, Dallmeijer AJ. Ambulatory activity of children with cerebral palsy: which characteristics are important? *Dev Med Child Neurol*. 2012;54(5):436-442. doi:10.1111/j.1469-8749.2012.04251.x

## SUPPLEMENT.

**eMethods.** Motor Assessment of Children with Deficits

**eReferences.**

**eTable.** Referent Accelerometry Data of Typically Developing Cohort

**eFigure 1.** Variance of Activity Over Time

**eFigure 2.** Most Common Daily Activities of Typically Developing Children Older Than 5 Years

**eFigure 3.** Causes Associated With Motor Deficits in Cohort